

32 solvent is evaporated with, or sometimes without, the application of heat. Among the
33 biopolymers seen as candidates for preparing these films are some polysaccharides, such as
34 starch (Bonilla et al., 2013; Dang and Yoksan, 2016; Nouri and Nafchi, 2014), and proteins, such
35 as the gelatine (Arfat et al., 2014; Etxabide et al., 2017; Tongnuanchan et al., 2014). Gelatine is
36 produced by the hydrolysis of animal collagen, so it can be obtained inexpensively from a wide
37 variety of sources. Furthermore, gelatine shows excellent biocompatibility, biodegradability
38 and non-toxicity and it can be used to prepare edible films capable of carrying different active
39 agents (Etxabide et al., 2017).

40 Among the active agents that have received the attention of the research community, thymol
41 can be highlighted due to its major antimicrobial properties. Thymol is obtained from essential
42 oils of plants of the family Lamiaceae, such as the genus *Thymus*, *Ocimum*, *Origanum*, *Satureja*,
43 *Thymbra* and *Monarda*. When pure, it is a crystalline substance with a characteristic scent.
44 Thymol and other compounds that are present in essential oils have been registered by the
45 Food and Drug Administration (FDA) as *Generally Recognised as Safe* (GRAS), and due to their
46 harmlessness and to their medicinal properties, they have also attracted the interest of the
47 food industry. However, thymol has some disadvantages that hinder its direct use in foods,
48 since it is a highly volatile compound, with low solubility in water and high solubility in ethanol
49 and other organic solvents and highly degraded by the light. Principally as a result of these
50 inconveniences, the incorporation of this active agent into edible films could be considered
51 problematic. If thymol is added to the film-forming solution, its low solubility in water could
52 lead to its aggregation during the solvent evaporation stage, producing a deterioration of the
53 film matrix, and therefore, a decrease in the mechanical properties of the films obtained. This
54 problem can be solved by solubilising the thymol in a solvent of high-ethanolic content, such as
55 that required to solubilise the protein zein. Films made with this protein and thymol have been
56 widely reported by several authors (Del Nobile et al., 2008; Li et al., 2012; Mastromatteo et al.,
57 2009; Park et al., 2012). Furthermore, during the solvent evaporation stage, the high volatility
58 of thymol could lead to its partial or total evaporation, a question that has scarcely been
59 investigated and which is of great interest when considering the possibility of introducing
60 thymol as an additive in protein-based films in order to take advantage of its desirable
61 properties. Kavooosi et al. (2013) produced gelatine films with thymol and in their study the
62 mechanical properties of the film were reinforced using glutaraldehyde, a toxic crosslinker that
63 cannot be allowed to come into contact with food. Despite the use of this crosslinker, the
64 addition of thymol produced a noticeable decrease in the mechanical properties of the film.

65 In recent research, Marcet et al. (2018) described the preparation and characterisation of
66 polylactic acid (PLA) nanoparticles loaded with thymol. PLA is a biodegradable and
67 biocompatible polymer that has been used by several authors to encapsulate other natural
68 antioxidants from plants, such as vanillin (Dalmolin et al., 2016) or aureusidin (Roussaki et al.,
69 2014). The addition of these nanoparticles loaded with thymol to the film-forming solution of a
70 protein-based film could solve two problems: first of all, it could potentially hinder the loss of
71 thymol during the evaporation step and furthermore, it might avoid the structural changes in
72 the film matrix caused by the active agent when it is free in the solution.

73

74 So, in this investigation, the PLA nanoparticles loaded with thymol that were reported in
75 previous work (Marcet et al., 2018) were incorporated into gelatine films. The amount of
76 thymol that remained in the film matrix after the film-forming solution drying step, the
77 mechanical properties, microstructure, thymol release behaviour and antioxidant properties of
78 these gelatine films were evaluated. Furthermore, the antimicrobial properties of the films
79 obtained were tested using apple pieces previously inoculated with *Escherichia coli*.

80

81 **2. MATERIALS AND METHODS**

82 **2.1. Materials**

83 The following reagents were acquired from Sigma-Aldrich (St Louis, USA): thymol (ref. T0501),
84 gelatine from porcine skin (ref. G1890), glycerol (ref. G7893), magnesium nitrate (ref. 237175).
85 The Nutrient Broth (NB, ref. 70149NB) and ethanol 96% (ref.83804.360) were acquired from
86 VWR (Pennsylvania, USA).

87 **2.2. Preparation of PLA nanoparticles loaded with thymol**

88 The PLA nanoparticles loaded with thymol were prepared using the single emulsion
89 preparation technique, a procedure reported in previous work (Marcet et al., 2018). This
90 previous study showed that the nanoparticles able to encapsulate the highest amount of
91 active agent were those prepared by dissolving 150 mg of thymol and 150 mg of PLA in 7.5 mL
92 of dichloromethane. This solution was then emulsified by ultrasound in 30 mL of a polyvinyl
93 alcohol solution. The nanoparticles thus prepared were spherical in shape and had an average
94 size of 244.6 ± 4.5 nm.

95

96 **2.3. Film preparation**

97 A stock solution of gelatine from porcine skin 6% (w/v) in distilled water was prepared. For
98 that purpose, the gelatine-water mixture was heated in a water bath at 65 °C for 25 minutes.
99 Then, an amount of glycerol equivalent to 30% (w/w) of the gelatine powder previously
100 dissolved was added, and the resulting solution was cooled at room temperature to 35 °C.
101 With this stock were prepared several film-forming solutions that contained 1%, 2% and 3%
102 (w/w of gelatine) of free thymol or alternatively of encapsulated thymol. These film-forming
103 solutions were poured into Petri dishes of 4 cm diameter in such a way that every film was
104 made up of 216 mg of gelatine, and then dried at room temperature for 2 days. Finally, the
105 films were manually peeled from the dishes. The films obtained were conditioned for 1 day at
106 room temperature (21 °C) in a closed chamber that contained a saturated solution of
107 $Mg(NO_3)_2$.

108

109 **2.4. Light absorbance, transparency, thickness and thymol content**

110 Light absorbance and transparency were determined according to Dick et al. (2015) using a
111 spectrophotometer (Spekol 1500, Analytik Jena AG, Jena, Germany) at selected wavelengths
112 between 200 to 800 nm. For this purpose, rectangular pieces of film were placed in the
113 spectrophotometer test cell, while an empty cell was used as reference. The transparency of
114 the films was calculated according to the following equation:

$$115 \text{ Transparency} = A_{600}/Th \quad (1)$$

116 Where A_{600} is the absorbance of the film sample at 600 nm and Th is the film thickness (mm).

117 The film thickness was measured using a digital micrometre (Model MDC-25PX, Mitutoyo C.,
118 Kanagawa, Japan), with a measuring range of 0-25 mm and a precision of $\pm 1 \mu m$. The film
119 thickness was measured in five different areas, one of them in the centre of the film and the
120 other four around the film perimeter.

121 To check the amount of thymol that remained in the films after the solvent evaporation of the
122 film-forming solution, a preliminary thymol release assay was performed to determine the
123 time required for all the thymol contained in the films to be released into an ethanol solution
124 (96%). Ethanol was selected for this experiment to ensure the diffusion of thymol, which is
125 highly soluble in this solvent. For that purpose, every type of film produced was placed in an
126 amber vial, filled with ethanol at 40 °C under orbital stirring for 72 hours. To calculate the

127 amount of thymol in the ethanol, an aliquot of 2 mL for each vial was taken at several times
128 and the absorbance at 275 nm was measured. The thymol concentration in the sample was
129 determined by preparing a calibration curve with known concentrations of thymol in ethanol.
130 The possible interferences produced by the film matrix were corrected using films without
131 thymol as blank. The amount of thymol released at 40 °C after 24 hours was considered to be
132 all the thymol contained in the films. The amount of thymol released into the ethanol was
133 compared with the amount of thymol incorporated into the film-forming solution to calculate
134 the thymol loss during the drying step.

135

136 **2.5. Mechanical properties of the gelatine films**

137 The measurement of the puncture strength (PS) and puncture deformation (PD) of the gelatine
138 films was carried out using a Texture Analyser TA.XT.plus (Stable Microsystems, Surrey, UK)
139 equipped with a load cell of 5 kg and a probe of 5 mm diameter (P/5S). For this purpose, the
140 films were cut into strips of 40 x 20 mm and attached in the assay platform between two
141 plates. Through the two plates a hole of 1 cm allows contact between the probe and the film
142 sample, so that the probe can stretch the film until it breaks. The probe velocity was 1 mm s⁻¹
143 and the PS and PD parameters were calculated according to the following equations (Pérez-
144 Mateos et al., 2009) :

$$145 \quad PS = F_m/Th \quad (2)$$

$$146 \quad PD = (\sqrt{D^2 + R^2} - R)/R \quad (3)$$

147 Where F_m is the maximum force applied before the film breaks, Th is the film thickness, D is
148 the distance covered by the probe while it is in contact with the film until the film is broken
149 and R is the radius of the orifice in the plates.

150 **2.6. Thymol release from gelatine films loaded with PLA nanoparticles**

151 The thymol released from the gelatine films into the liquid medium was evaluated in
152 accordance with ASTM D4754-98 (ASTM, 2006). In this case only the films loaded with PLA-
153 thymol nanoparticles were evaluated, and the release of the thymol was carried out at three
154 different temperatures (5 °C, 20 °C and 40 °C), using ethanol (96%) as the food simulant.
155 Ethanol has been commonly used as a fatty food simulant by other authors to study the
156 release of different non-water soluble active agents from films (Manzanarez-López et al., 2011;
157 Ortiz-Vazquez et al., 2011; Rodríguez-Martínez et al., 2016). For this purpose, each film tested

158 was cut into four round discs (2 cm of diameter). These four discs were immobilized using a
159 stainless-steel wire and separated one from another using glass beads of 5 mm diameter.
160 Then, the film pieces were placed in amber vials that were filled with 20 mL of ethanol. The
161 ethanol volume/film area was 0.8 mL cm^{-2} , which is within the volume-to-surface area range,
162 from 155 to 0.31 mL cm^{-2} , recommended by the ASTM D4754-98. The release of thymol from
163 the films to the liquid medium was measured at several times, using the technique explained
164 in section 2.4. After every measurement, the ethanol sample was returned to the vials.

165 To calculate the diffusion coefficient of the thymol (D), the analytical solution of Crank (1979)
166 (equation 4) to study the diffusion phenomena in a plane sheet was used. To apply this
167 equation, it was assumed there was no reaction between thymol and the film matrix, a
168 homogeneous concentration distribution of thymol, that the amount of solvent can be
169 considered infinite, negligible edge effect, and therefore a unidirectional diffusion of the active
170 agent from the surface of the film into the liquid).

$$171 \quad \frac{M_t}{M_\infty} = 1 - \sum_{n=0}^{\infty} \frac{8}{(2n+1)^2 \pi^2} e^{\{-D(2n+1)^2 \pi^2 t / 4L^2\}} \quad (4)$$

172 Where M_t is the amount of thymol released at each time, M_∞ is the amount of thymol released
173 after infinite time and L is the half-thickness of the films tested. If instead of considering all the
174 data collected during this experiment, only the values of $M_t/M_\infty > 0.4$ are taken, equation 4 can
175 be rewritten as the following linear regression model (Han et al., 2000):

$$176 \quad \ln \left(1 - \frac{M_t}{M_\infty} \right) = \ln \frac{8}{\pi^2} - \frac{D\pi^2 t}{4L^2} \quad (5)$$

177 When the first term of this equation is plotted vs time, the D parameter can be calculated from
178 the slope.

179 To assess the dependence of the thymol diffusion on temperature, the activation energy (E_a)
180 was calculated. For that purpose, the Arrhenius model was applied using the D values obtained
181 from equation (5) (Limm and Hollifield, 1996):

$$182 \quad \ln D = \ln D_0 - \frac{E_a}{RT} \quad (6)$$

183 Where D_0 is a constant, T is the temperature tested (K) and R is the universal gas constant.

184

185 **2.7. Scanning electron microscopy**

186 The micrographs of the transversal section of the films were performed according to Kadam et
187 al. (2015) and using a scanning electron microscope (JSM-6610LV, JEOL, Tokyo, Japan). To

188 obtain these micrographs, the films were lyophilized and cut into 1x1 cm squares. These
189 samples were mounted perpendicularly on aluminium stubs and covered with gold. The
190 microscope was operated with a voltage of 20 kV.

191 **2.8. Antimicrobial properties of the gelatine films**

192 To test the antimicrobial properties of the gelatine films with thymol and the nanoparticles
193 loaded with thymol, 1 g pieces of apple (Royal Gala apple variety) were inoculated with the
194 non-pathogenic strain of *E. coli* CECT 101 (CECT, *Colección Española de Cultivos Tipo*, Spanish
195 Type Culture Collection). This strain was cultured using NB (Nutrient Broth) medium,
196 supplemented with 2% agar and incubated at 30 °C for 48 hours. It was then incubated in NB
197 liquid for 10 hours at 30 °C under orbital stirring at 26.17 rad s⁻¹.

198 The apple pieces were inoculated with 0.1 mL of this solution, containing an *E. coli*
199 concentration of 10⁵ CFU mL⁻¹. These apple pieces were then covered with the gelatine films
200 and sealed using a heat-sealing machine. Every piece of apple sealed was placed in a petri dish
201 and stored at 5 °C for 14 days. To follow the growth of *E. coli* with each type of gelatine film
202 tested, after 3 or 4 days of storage time a sample was taken, the film removed, the apple
203 mixed with 9 mL of NaCl 0.7% and the mixture triturated using a Stomacher (IUL Instruments,
204 Barcelona, Spain) for 120 seconds. Then, the liquid sample obtained was diluted and seeded in
205 NB medium with 2% agar. After 24 hours of incubation at 30 °C the colonies were counted and
206 expressed as log₁₀ CFU mL⁻¹.

207 **2.9. Statistical analysis**

208 Experiments were performed in triplicate and are shown as the mean value ± standard
209 deviation of three independent experiments (n = 3). Least significant differences (LSD) were
210 calculated by Fisher's test to determine significant differences between the tested samples.
211 These analyses were performed using the statistical software Statgraphics® V.15.2.06.

212 **3. RESULTS**

213 **3.1. Light absorbance, transparency, thickness and thymol content**

214 After the solvent evaporation of the film-forming solution for 2 days, the films were peeled
215 easily and entirely, not showing a sticky or brittle appearance. The visual aspect of the films is
216 shown in Figure 1. The gelatine films with free thymol are not shown because their appearance
217 was identical to that of the control films. In this Figure it can be observed how the increment in
218 the amount of PLA nanoparticles produced a decrease in the film transparency. This variation
219 in the transparency parameter was also noticed when the film strips were analysed using the

220 spectrophotometer (Table 1), a rise from 0.48 in the control films to 1.04 in the films with 3%
221 thymol encapsulated in PLA nanoparticles being detected. It is understood that a rise in this
222 value corresponds to a decrease in the film transparency.

223 Regarding the absorbance values at different wavelengths, is also desirable that a good film
224 can act as a barrier to ultraviolet light, since this is an important starter for the lipid oxidation
225 process (Coupland and McClements, 1996). Most protein-based films have a high capacity to
226 absorb ultraviolet light, due to the presence of amino acids with aromatic side chains, such as
227 tyrosine, tryptophan and phenylalanine. However, the gelatine protein lacks tryptophan and it
228 has a fairly low amount of tyrosine and phenylalanine (Nhari et al., 2011). This results in a
229 relatively low barrier capacity at these wavelengths for the gelatine films in comparison with
230 other protein-based films. Table 1 shows that the control films present an absorbance at 280
231 nm of 0.808, whereas the gelatine film with 3% thymol in nanoparticles has an absorbance of
232 1.521, which is a rise of 0.71. Taking into account that PLA does not show particularly high
233 absorbance at this wavelength, this increase could be produced by the addition of thymol,
234 which exhibits an absorption spectrum with a major peak at 274 nm (Hajimehdipoor et al.,
235 2010). Furthermore, the gelatine films with 3% free thymol showed an absorption profile
236 similar to that found for the control film, which suggests the total evaporation of the thymol
237 during the film-forming solvent evaporation step. The gelatine films with 2% and 1% free
238 thymol showed the same absorbance value as that found for the gelatine film with 3% free
239 thymol.

240 With respect to the thickness, a slight increase was detected when the nanoparticles were
241 added, in particular, when the thickness value for the control films is compared with the value
242 for the 3% nanoparticles gelatine films (Table 1). The addition of free thymol to the film-
243 forming solution produced films with the same thickness value as that of the control films.

244

245 The film transparency, absorbance at 280 nm and thickness values obtained suggest that all
246 the free thymol incorporated into the gelatine films was evaporated during the drying of the
247 film-forming solution. This supposition was confirmed when the amount of thymol in these
248 films was tested (Table 1). Films with 3% free thymol lost all their active agent content during
249 the solvent evaporation step. This could be explained by both the high volatility of thymol and
250 the low capacity of gelatine to retain the thymol molecules. In the case of proteins, molecular
251 binding studies carried out by Pan et al. (2014) showed that thymol is able to bind to tyrosine
252 and tryptophan residues in a protein, but as was mentioned previously, the former amino acid

253 is found at a very low proportion in gelatine, and the latter is not present at all, due to it is
254 being degraded during the production of the gelatine (Hafidz et al., 2011). In addition, when
255 thymol encapsulated in PLA nanoparticles was incorporated into the film-forming solution, the
256 thymol loss was also noticeable, but a proportion of the added thymol remained in the dried
257 film (Table 1). It is to be expected that during the drying of the film-forming solution a part of
258 the thymol in the nanoparticles is continuously diffusing into the aqueous medium and is then
259 evaporated together with the solvent. This effect is likely to be enhanced at the beginning of
260 the drying step, when the amount of water in the film-forming solution is large enough to
261 produce a major release of thymol from the nanoparticles to the water.

262 Taking into account the total evaporation of the free thymol in the gelatine films during the
263 film-forming solution drying step, in the following experiments only the gelatine films loaded
264 with PLA-thymol nanoparticles were considered.

265

266 **3.2. Gelatine films: mechanical properties**

267 The PS and PD values of the gelatine films are shown in Figure 2. The PS parameter indicates
268 the mechanical resistance of a film, and in this case, the addition of nanoparticles loaded with
269 thymol did not produce any statistically significant variation ($p < 0.05$). Furthermore, the PD
270 parameter, which is a measurement of the film's elasticity, was influenced by the addition of
271 PLA nanoparticles, a statistically significant difference appearing between the control film and
272 those with 2% and 3% thymol in PLA nanoparticles. During the film drying, the protein chains
273 come closer and establish non-covalent interactions with one another. In this type of film, the
274 glycerol and water avoid the excessive structuration of the film matrix, allowing some degree
275 of flexibility. In this case, nanoparticles could be occupying places within the film matrix where
276 the glycerol and the water had previously accumulated, replacing them and leading to a
277 decrease in the flexibility of the material. In any case, the decrease in the PD parameter due to
278 the addition of the nanoparticles could be considered slight, from $37.2 \pm 7.0\%$ in the control
279 film to $26.5 \pm 6.2\%$ in the case of the gelatine film with 3% thymol in nanoparticles.

280 **3.3. Scanning electron microscopy**

281 The micrographs of the film matrix are shown in Figure 3. In these micrographs it can be
282 observed how the films showed a highly homogeneous transverse section, even in the case of
283 the gelatine films with 3% thymol encapsulated in nanoparticles. However, the smoothest
284 cross section area was that found for the gelatine control film, and a slight decrease in this

285 homogeneity can be observed as the amount of encapsulated thymol increased. This slight
286 difference between the micrographs shown in Figure 3D and 3A could explain the loss of
287 elasticity that was appreciated when the mechanical properties of the films were tested.

288 **3.4. Thymol release from gelatine films loaded with PLA-thymol nanoparticles**

289 The thymol release profiles for the gelatine films with different thymol-loaded nanoparticle
290 concentrations were very similar to each other at every temperature tested, regardless of the
291 amount of thymol incorporated into the films (Figure 4). Furthermore, changes in temperature
292 produced variations in the shape of the curves for the three thymol concentrations tested, as
293 was expected. In particular, at 40 °C, all the thymol contained in the nanoparticles was
294 released in two hours independently of the concentration of thymol. At 20 °C, almost all the
295 thymol was released in 23 hours, and at 5 °C all the thymol incorporated was released in 71
296 hours. The differences in the shape of the thymol release profiles at each temperature tested
297 could be mainly due to the effect of the temperature on thymol solubility. So, at 40.4 °C the
298 thymol solubility value is 946 mg mL⁻¹, while at 30.9 °C this value decreases to 744 mg mL⁻¹
299 (Villanueva Bermejo et al., 2015). The diffusion coefficients calculated using equation (5) for
300 these release curves are shown in Table 2. The experimental data obtained fitted to this
301 equation with a high coefficient of determination ($R^2 > 0.99$). As is shown in this Table, the
302 value of these coefficients decreased by a similar degree from 40 °C to 20 °C as from 20 °C to 5
303 °C, which suggests that the temperature does not affect the thymol release mechanism, and
304 that the drop in the thymol release rate is caused mainly by a decrease in thymol solubility.
305 Furthermore, the diffusion coefficient decreased by one order of magnitude when the
306 temperature fell from 40 °C to 5 °C, which was also seen by other authors working with thymol
307 and zein films (Kashiri et al., 2017). In addition, similar diffusion values to those shown in Table
308 2 were reported by Ramos et al. (2014), studying thymol release from polypropylene films
309 using ethanol 95% as food simulant and at 40 °C. In this case, these authors reported a
310 diffusion coefficient of $1.01 \times 10^{-10} \text{ cm}^2 \text{ s}^{-1}$.

311 To study the temperature dependence of the diffusion values obtained, an Arrhenius plot was
312 carried out (Figure 5). The diffusion values shown in Table 2 were fitted to the Arrhenius
313 equation with a high coefficient of determination ($R^2 > 0.99$), which suggest that the diffusion
314 of encapsulated thymol into the gelatine films can be explained by the Arrhenius activation
315 model. Therefore, the diffusion process is driven mainly by the amount of energy provided to
316 the medium, with no structural modification in the film matrix due to the temperature
317 involved. The activation energies calculated from Figure 5 are shown in Table 2, and as was

318 expected, variations in the concentration of encapsulated thymol added to the films did not
319 produce a great variation in the value of this parameter.

320

321 **3.5. Antimicrobial capacity of the gelatine films loaded with thymol**

322 The effect of the gelatine films with PLA nanoparticles loaded with thymol is shown in Figure 6.

323 Films loaded with encapsulated thymol at 3% and 2% exhibited a similar, low antimicrobial
324 capacity during the first 3 days of storage, but at the sixth day the difference between these
325 two samples was noticeable: the gelatine films loaded with 3% encapsulated thymol decreased
326 the CFU g⁻¹ value to 1.95, while in the case of the films loaded with 2% encapsulated thymol,
327 the CFU g⁻¹ value decreased to 3.9. During the following days, the decrease in the CFU value
328 was more pronounced in the 2% films, whilst it remained relatively constant for the 3% film. At
329 the end of the storage time, a CFU g⁻¹ value of 2.0 was found for the 2% films, while a decrease
330 to 1.5 CFU g⁻¹ was measured for the 3% films. It should be expected that the release of thymol
331 from the film to the surface of a food with a relatively high-water content, such as a piece of
332 apple, will be slower than the relatively fast release of thymol to ethanol shown in section 3.4.
333 The reason for this difference in diffusivity is mainly due to the low solubility of thymol in
334 water. This long-term effect is desirable and could explain the reduction in CFUs after 6 days of
335 storage for the pieces of apple covered with 3% and 2% PLA-thymol nanoparticles gelatine
336 films. The antimicrobial effect of the PLA-thymol nanoparticles on *E. coli*-inoculated pieces of
337 apple was tested in a recent study (Marcet et al., 2018), and these antimicrobial properties
338 were found to be slightly worse than those shown by the gelatine films loaded with the same
339 nanoparticles. In the case of the PLA-thymol nanoparticles without film, the amount of thymol
340 encapsulated was 0.5 mg mL⁻¹ in the case of the best result obtained, while the concentration
341 of thymol in the PLA-thymol nanoparticles included in the gelatine films was higher than that
342 measured in the PLA-thymol nanoparticles without film, even taking into consideration the
343 evaporation of thymol during the film-forming solution drying step. This could explain the
344 better antimicrobial capacity observed when the PLA-thymol nanoparticles were incorporated
345 into films.

346

347 **4. CONCLUSIONS**

348 The amount of thymol evaporated during the production of protein-based films is a subject
349 that has barely been addressed in this type of packaging materials, and it could have a major

350 impact on the costs associated with their production, especially considering that this problem
351 is likely to be common to the use of other volatile essential oils. In this study, the total
352 evaporation of non-encapsulated thymol from the gelatine films during the drying step could
353 be due to both to the relatively low amount of thymol added to the film-forming solution and
354 also to the particular amino acid composition of the gelatine proteins; the former is
355 recommendable, since it reduces the weakening effect exerted by the thymol on the
356 mechanical properties of the films, and the latter is very difficult to avoid. In any case, the
357 incorporation of thymol in the form of PLA-thymol nanoparticles in the film-forming solution
358 resulted in the production of solid gelatine films with the active agent present in the film
359 matrix. This thymol that remains in the film matrix showed antimicrobial properties, and its
360 impact on the mechanical properties of the materials produced can be considered slight.

361

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***Conflict of Interest form**

Conflict of Interest and Authorship Conformation Form

Please check the following as appropriate:

- All authors have participated in conception and design, or analysis and interpretation of the data; drafting the article or revising it critically for important intellectual content; and approval of the final version.
- This manuscript has not been submitted to, nor is under review at, another journal or other publishing venue.
- The authors have no affiliation with any organization with a direct or indirect financial interest in the subject matter discussed in the manuscript

Figure 1.

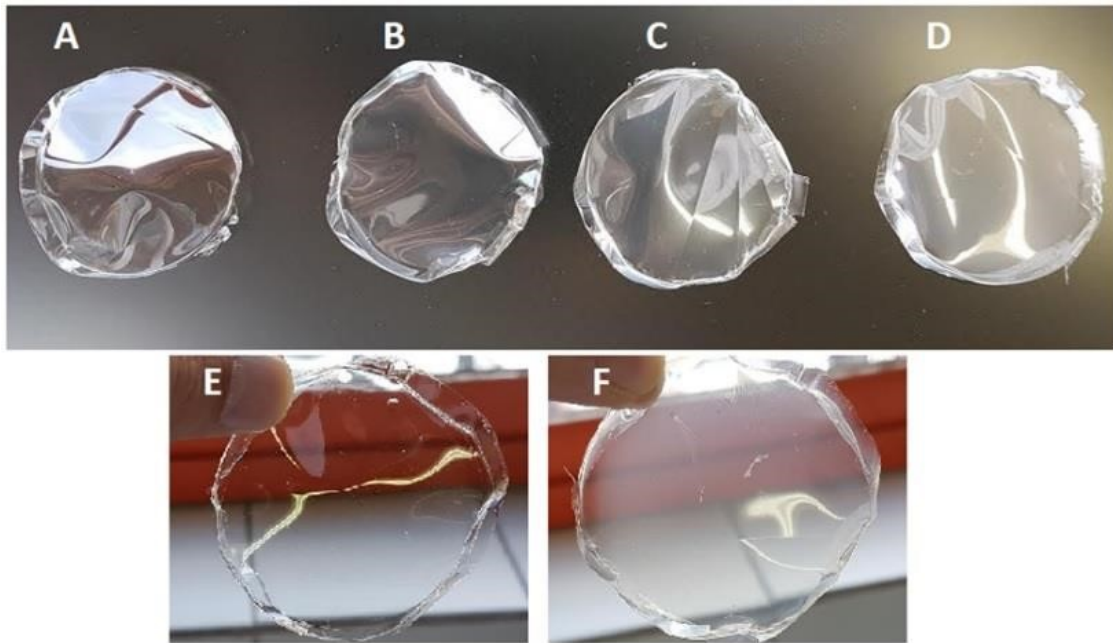


Figure 2.

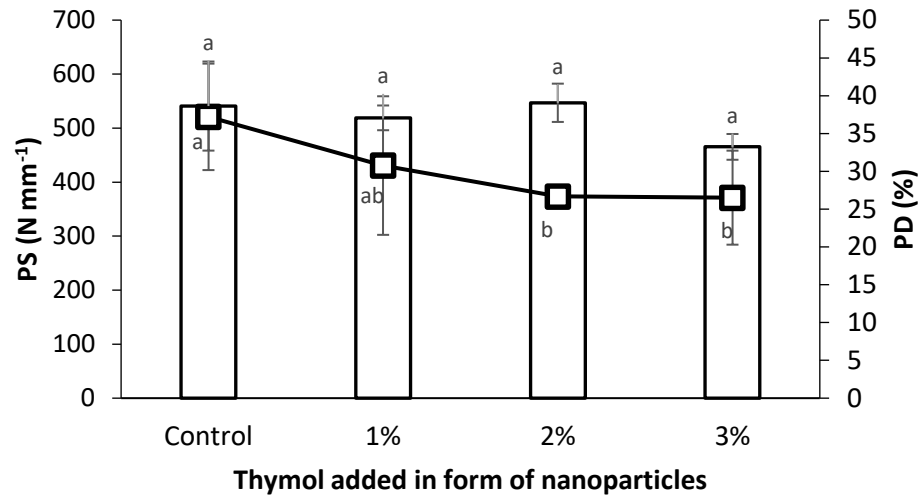


Figure 3.

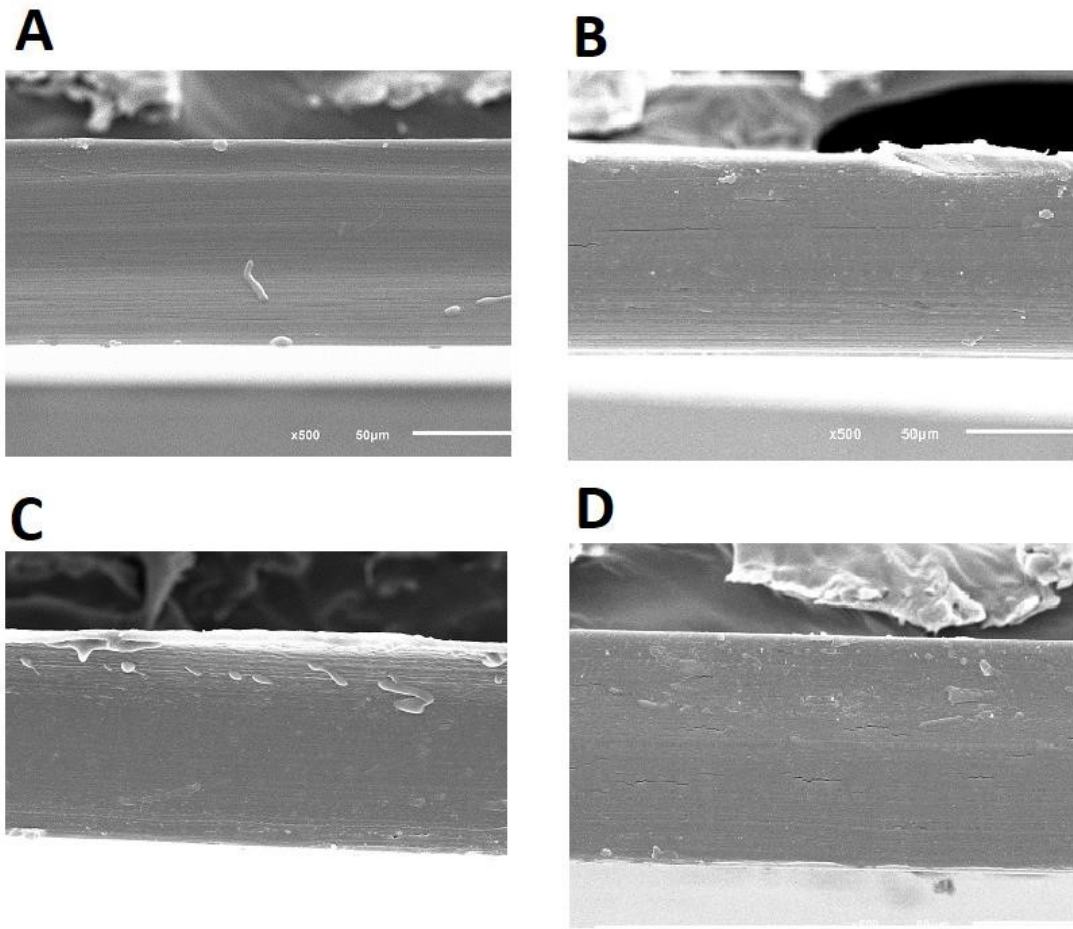


Figure 4

Figure 4.

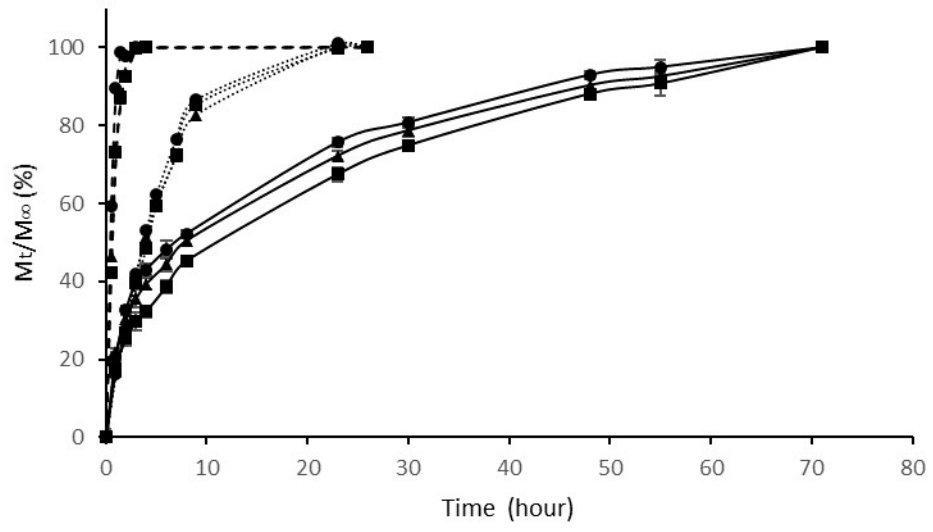


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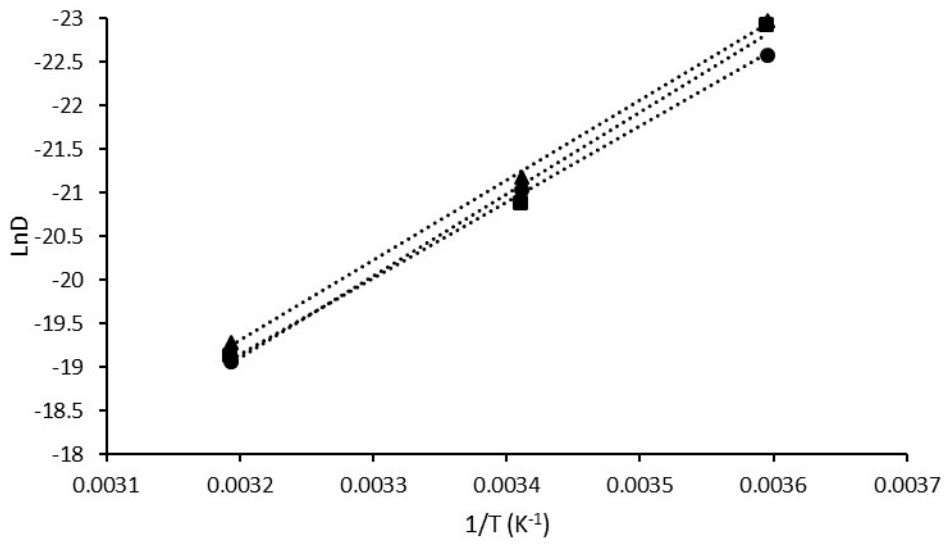


Figure 6.

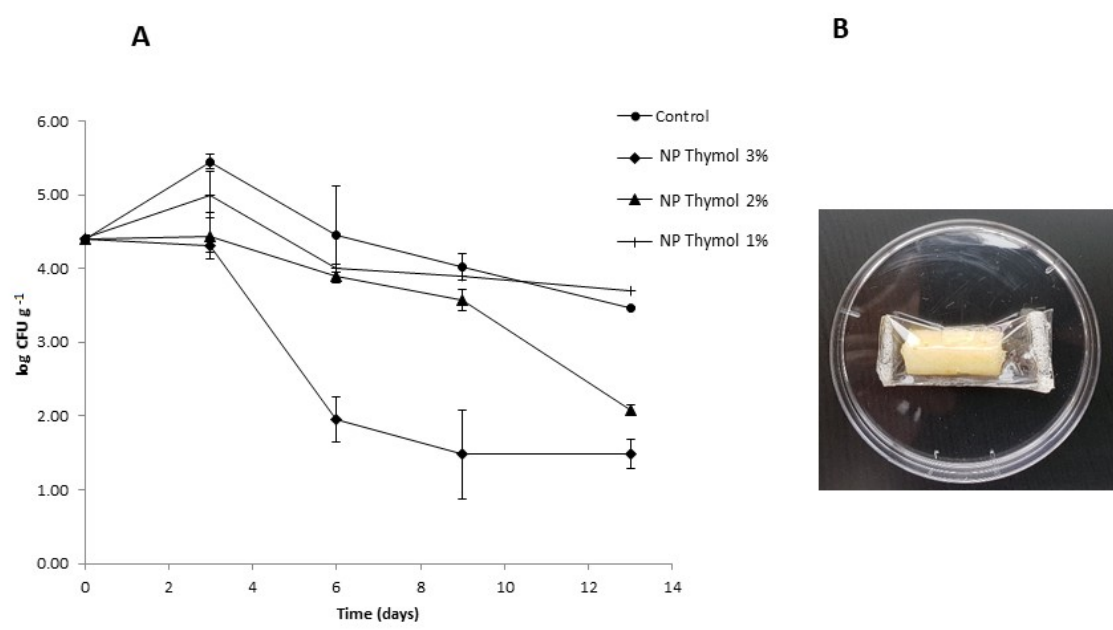


Figure Captions

Figure 1. Visual appearance of the films obtained. A and E. Gelatine films control, without the addition of thymol. B. Gelatine film with 1% of thymol encapsulated in nanoparticles. C. Gelatine film with 2% of thymol encapsulated in nanoparticles. D and F. Gelatine film with 3% thymol encapsulated in nanoparticles

Figure 2. Mechanical properties of the tested films. PS parameter is represented with bars, while PD is represented with squares. For each parameter, different letters indicate statistically significant difference ($p < 0.05$).

Figure 3. Micrographs of the transverse section of the gelatine films loaded with PLA-thymol nanoparticles at 500x. A. Control film. B. Gelatine film with 1% thymol. C. Gelatine film with 2% thymol. D. Gelatine film with 3% thymol

Figure 4. Diffusion kinetics of thymol in gelatine films loaded with PLA-thymol nanoparticles. Broken line, 40 °C. Dotted line, 20 °C. Continuous line, 5 °C. Circles, gelatine film with 1% thymol. Triangle shape, gelatine film with 2% thymol. Squares, gelatine film with 3% thymol.

Figure 5. Arrhenius plot for the release of thymol from the gelatine films with thymol encapsulated in nanoparticles. Circles, gelatine film with 1% thymol. Triangle shape, gelatine film with 2% thymol. Squares, gelatine film with 3% thymol.

Figure 6. A. Growth of *E. coli* CECT 101 on apples covered with gelatine films that have PLA-thymol nanoparticles incorporated. B. Sample of apple piece covered with a gelatine film that has a 3% PLA-thymol nanoparticle content.

Table 1

Table 1. Film thickness, transparency, absorbance at different wavelengths and amounts of thymol remaining after the drying of the film-forming solution.

	Thickness (mm)	Absorbance									Transparency	Thymol that remains in the film (%)
		200 nm	250 nm	280 nm	300 nm	400 nm	500 nm	600 nm	700 nm	800 nm		
Control	0.094 ± 0.007 ^a	2.407	0.894	0.808	0.181	0.056	0.046	0.045	0.044	0.043	0.48	--
NP 1%	0.102 ± 0.002 ^{ab}	> 3.0	1.147	1.059	0.289	0.112	0.085	0.072	0.065	0.064	0.71	11.6 ± 0.7 ^a
NP 2%	0.102 ± 0.003 ^{ab}	> 3.0	1.198	1.189	0.323	0.132	0.099	0.083	0.075	0.069	0.81	14.3 ± 1.0 ^b
NP 3%	0.110 ± 0.003 ^b	2.846	1.496	1.521	0.452	0.196	0.142	0.115	0.102	0.09	1.04	18.5 ± 1.2 ^c
Thymol free 3%	0.096 ± 0.005 ^a	2.455	0.880	0.838	0.191	0.058	0.045	0.045	0.044	0.043	0.46	0

Different letters in the same column indicate significant differences (P<0.05).

Table 2. Diffusion coefficients of thymol released from gelatine films loaded with PLA-thymol nanoparticles into ethanol at 5, 20 and 40 °C, and activation energies for the diffusion of thymol from the gelatine films.

Films with nanoparticles loaded with thymol	Diffusion coefficients (cm ² s ⁻¹)			Activation Energies (KJ mol ⁻¹)
	5 °C	20 °C	40 °C	
3%	1.10 (x 10 ⁻¹⁰)	8.60 (x 10 ⁻¹⁰)	4.90 (x 10 ⁻⁹)	78.13
2%	1.05 (x 10 ⁻¹⁰)	6.33 (x 10 ⁻¹⁰)	4.22 (x 10 ⁻⁹)	76.20
1%	1.58 (x 10 ⁻¹⁰)	7.38 (x 10 ⁻¹⁰)	5.27 (x 10 ⁻⁹)	72.62